

Forearm Bio-Medical Signal Processing

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Abstract

This research utilizes low-dimensional surface EMG and EEG data, obtained from the human arm using ECG electrodes, to analyze forearm muscle signals through a novel approach. Both EMG and EEG signals are employed side by side: EEG captures brain activity, particularly in the beta (13-30 Hz) and alpha (8-12 Hz) frequency ranges, while EMG focuses on muscle activity in the 20 Hz to 200 Hz range. Beta waves are associated with motor planning and voluntary movements, while alpha waves decrease during movement execution, indicating disengagement from a resting state. Event-related desynchronization (ERD) of alpha and beta waves is vital in understanding motor tasks, including forearm movements. Although EEG alone showed a poor response in tracking movement execution, EMG provided better performance, with higher frequencies reflecting more intense muscle contractions and motor unit activation. The combination of EEG and EMG improves the analysis of event-related potentials (ERPs) in timing tasks, enabling precise monitoring of both brain and muscle activity. However, coordinating both signals can be complex and often relies on user experience. Extensive experimentation confirms that using this dual approach is feasible and effective in replicating natural arm movements. The findings highlight important advancements in applying signal processing techniques to muscle activity analysis, providing new insights into the control of muscles and enhancing accessibility to modern assistive technologies.

Keywords: EMG, robotic arm, EEG, ERP, CNN, PCA

1. Introduction

This work focuses on the processing and analysis of bio medical signals in order to create a biofeedback system that can be used to operate a mechanical arm. The apparatus utilizes data obtained from electrodes positioned on three different upper limb muscle groups. Because signals are low amplitude and intrinsically noisy, specific filters and amplifiers are used to guarantee dependable signal acquisition and processing. These preparatory procedures are essential for producing dependable control signals that enable accurate mechanical arm movement. Before the raw data from the electrodes is analyzed, the system is trained using the MEG III clinical dataset (GRABMyo open access Dataset) to improve its accuracy. The main goal is to translate the acquired data into commands that may be used to control particular movements, such gripping or spinning. This method seeks to provide intuitive and responsive control by mapping specific patterns to related motions. This biofeedback system has potential applications in industrial settings requiring precise equipment management in both normal and hazardous conditions, in addition to its usage in medical rehabilitation. This work explores broader applications in multiple sectors and provides enhanced mobility and utility for those with upper limb constraints, marking a substantial advancement in biological signal analysis.

2. Related Works

The paper "Brain EEG Signal Processing for Controlling a Robotic Arm" by Howida A. Shedeed, Mohamed F.

Issa, and Salah M. El-sayed, published in IEEE, explores the application of EEG (Electroencephalography) signals for enhancing the control of robotic prosthetic arms. By employing specialized electrodes and amplifiers, the methodology first acquires EEG signals. To enhance signal clarity, preprocessing techniques such as noise reduction and artifact removal are applied. From EEG data, feature extraction techniques detect pertinent patterns, which are then translated into precise control commands (e.g., grip, rotate) by classification algorithms like Support Vector Machines (SVM) and Neural Networks. Experimental results reveal that EEG-based control is feasible and practical, with short response times, resilient performance under many situations, and high classification accuracy. User studies offer valuable perspectives on usability and acceptance, disclosing affirmative responses about the intuitiveness of EEG-controlled prosthetics. In conclusion, the study addresses issues such as signal variability and the need for real-time processing capabilities, and it offers recommendations for future research approaches. The paper goes on to analyze signal variability and the necessity for real-time processing capabilities, and it also recommends future research topics, including hybrid EEG-EMG systems and advanced signal processing methods. By using EEG signals to improve prosthetic device function and user experience, the work promotes neurorehabilitation and assistive technology overall and may improve the quality of life for those with upper limb disability (Shedeed, 2013).

The paper "Design and Development of EMG Controlled Prosthetic Limb" dives into the complex engineering techniques required to create an EMG (Electromyography) controlled prosthetic limb. This new device aims to restore functionality to people who have lost or impaired their limbs by using EMG signals generated by remaining muscles in the user's limb. The study thoroughly examines the integration of advanced EMG sensors, complex signal processing algorithms, and responsive actuators into the prosthetic limb architecture. By recording and interpreting EMG signals, the prosthetic limb may perform intuitive and accurate motions that are similar to natural limb function. The paper addresses key aspects such as optimizing sensor placement for accurate signal acquisition, developing robust signal processing techniques to decode user intentions in real time, and implementing actuators capable of translating these decoded signals into coordinated movements. These technical advancements seek to improve prosthetic users' entire quality of life in addition to the functioning and performance of their prosthetic limbs. The interdisciplinary approach provided in this study emphasizes the collaboration of biomedical engineers, neuroscientists, and prosthetists in pushing the frontiers of assistive technology, opening the way for more natural and integrated prosthetic solutions in the future (Sudarsan & Sekaran, 2012).

In 'A Review of Myoelectric Control for Prosthetic Hand Manipulation,' Ziming Chen et al. offer a thorough examination of the myoelectric control methods utilized in prosthetic hands. It addresses advances in EMG signal processing and pattern recognition algorithms, which are critical for producing accurate and realistic motions. The paper discusses problems including signal variability and user adaptation and looks at how artificial intelligence (AI) and other cutting-edge technologies might improve prosthetic control systems. It is an excellent resource for academics and engineers working to create more effective prosthetic solutions (Chen, 2023).

3. Significance of the Research

This study aims to enhance the interpretation of forearm EMG and EEG data using advanced biomedical engineering techniques. Traditional methods often fall short in capturing the nuanced muscle and brain activity necessary for effective analysis, particularly for individuals with congenital disorders like acheiropody, which affects hand and arm functionality (MedlinePlus). By employing specialized filters and amplifiers, the research seeks to improve the quality of EMG signals, addressing low amplitude and inherent noise. Sophisticated signal processing techniques, including amplification, filtering, and pattern recognition, will enable a more accurate understanding of brain and muscle activity. This refined analysis could lead to more effective rehabilitation programs for those with neurological and muscular disabilities and the development of assistive devices that enhance the quality of life for individuals with limb disorders. The integration of EMG and EEG data marks a significant shift from traditional methods, fostering a user-centered approach that utilizes direct signals from the

user's muscles and brain. Ultimately, this research aims to revolutionize the design of assistive and performance-enhancing devices, improving occupational safety, productivity, and overall quality of life for individuals requiring enhanced physical capabilities and rehabilitation support (De Luca & Mambrito, 1987).

4. Background

4.1. Signal Acquisition System

ADC converts analog EMG signals $x(t)$ into digital format for computational analysis. The sampled signal $x[n]$ is obtained at discrete time intervals T_s .

4.2. Preamplification using Differential Amplifier

Preamplification with a differential amplifier is crucial for improving the quality of electromyography (EMG) data. EMG signals are intrinsically weak, ranging from microvolts to millivolts, and are sensitive to a variety of noise sources, including electrical interference and biological aberrations (Blackely, 2007). Differential amplifiers address these issues by raising the amplitude of EMG signals while reducing noise, resulting in an improved signal-to-noise ratio and signal fidelity.

$$V_{out} = G. (V_+ - V_-) \tag{Equation 1}$$

Where,

G is Gain

V_+ and V_- are voltages

4.3. Filtration

The Sallen Key filter is a versatile circuit that is widely employed in signal processing applications to effectively regulate and shape frequency responses, particularly in situations where accurate filtering of EMG signals is required, such as in bio robotic arms and prosthetic devices. This filter works well at reducing extraneous noise and separating the EMG signal's pertinent frequency components (Luca, 1997). A second-order Sallen Key low-pass filter's transfer function is mathematically described as follows:

$$H(S) = \frac{k}{s^2 + \frac{s}{Q} + \omega^2} \tag{Equation 2}$$

Where,

K is Gain

Q is the Quality Factor

ω is the natural frequency

4.4. Signal Processing Techniques

A wide range of techniques are included in signal processing methods for the manipulation, analysis, and interpretation of data. This includes images, audio, and biological signals like electromyography (EMG) used in bio-robotics applications. These techniques are critical for extracting relevant information, reducing noise, improving signal quality, and eventually making data more valuable for diverse applications (Blackely, 2007).

4.5. Machine Learning Approaches

Machine learning techniques, particularly Convolutional Neural Networks (CNNs) that use the sliding window

approach, have become essential in field of electromyography (EMG) signal processing for bio-robotic applications. One of the most significant advantages of using CNNs is their ability to automatically extract useful characteristics directly from raw EMG signals. Unlike older methods that necessitate human feature engineering, CNNs learn discriminative patterns through their convolutional layers, increasing the flexibility of bio robotic systems to varied users and environments. This automatic feature learning capability helps the development process while also improving the accuracy and robustness of gesture recognition and control systems in prosthetic limbs.

5. Methodology

The basic concept involves leveraging low-dimensional electromyography (EMG) and electroencephalography (EEG) data for advanced biomedical signal analysis. Signal Acquisition, Training and Developing the Machine Learning Model, Controller, and Signal Analysis are the four primary parts of the system. It can be further broken down into two main categories: using the dataset to build models and using those models to examine electrode raw data signals. To make the best use of EMG and EEG data, this integrated methodology combines advanced signal processing techniques with machine learning methodologies. Each stage, from initial signal analysis to feature extraction and predictive modeling, contributes to a better knowledge of the biological signals generated by the forearm. By focusing on EMG and EEG signal processing, this technology improves the ability to interpret muscle and brain activity patterns. These developments are critical for developing biomedical engineering applications, notably in understanding muscle function and neurological signaling. This study promotes the development of novel solutions that will improve clinical diagnosis, rehabilitation techniques.

5.1. Model Construction based on Dataset

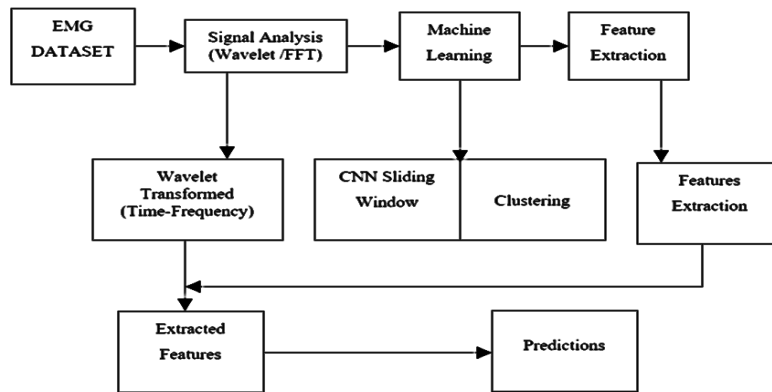


Figure 1. Block Diagram for Model Construction

5.1.1. Data Creation

The Dataset used for model construction is a meg III clinical dataset (GRABMyo open access Dataset) obtain from physionet. The dataset contains electrical signals collected from electrodes placed on the muscles of interest. These signals describe electrical activity produced by muscle fibers during contraction and relaxation. Each signal is a time series representing the amplitude and frequency of muscle activity

5.1.2. Signal Analysis

This approach splits the signal into temporal and frequency domains. It employs a wavelet function that is scaled and shifted over the signal to extract information at various scales. This enables thorough examination of how frequency components change over time, revealing changes in muscle activity patterns across various actions or

situations. The Fast Fourier Transform converts the signal from the time domain to the frequency domain (Kuriki, 2012).

5.1.3. Machine Learning Model

The sliding window approach divides the continuous signal into smaller frames with predetermined durations. Each segment is then fed into the CNN, which learns to identify discriminative features from the temporal data. This method allows the CNN to classify muscular gestures or motions based on learnt patterns inside each frame, making it ideal for real-time applications that require immediate feedback. K-means methods are used to group segmented signal frames. These algorithms group comparable segments together based on pattern similarity and do not require labeled data. Clustering improves our understanding of muscle activation patterns by identifying shared patterns across people or situations. It helps group data into discrete clusters, each of which corresponds to a particular kind of movement or muscle activity.

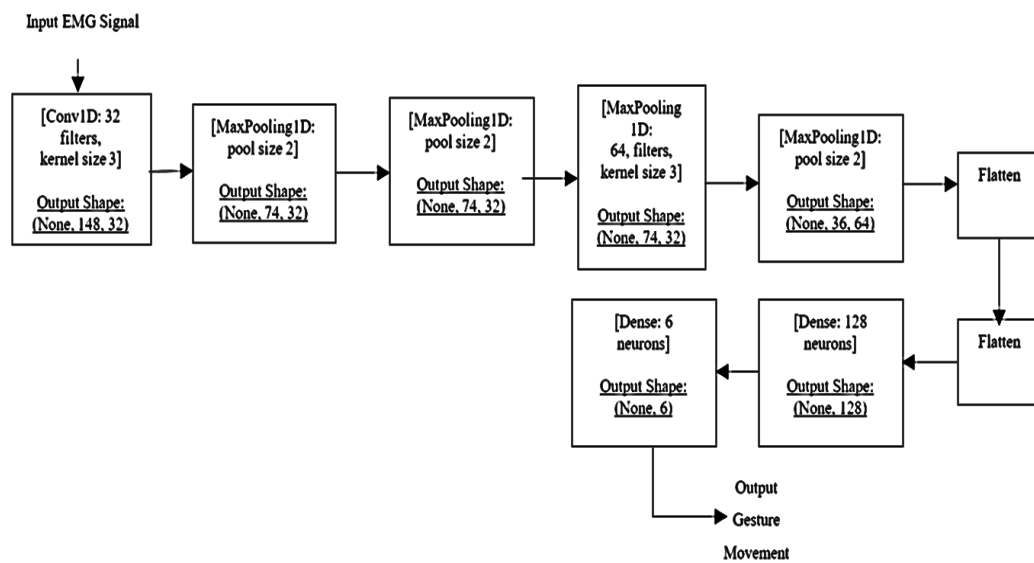


Figure 2. CNN Architecture for the model

5.1.4. Features Extraction

Feature extraction aims to extract relevant and discriminative qualities from processed signal data. These properties can be statistical measures, frequency domain features, or time-domain features (Merletti, n.d). Extracted features are critical for subsequent prediction tasks because they reduce complex data for accurate classification.

5.1.5. Prediction

Using the collected features, the final stage is to forecast muscular gestures or movements. Machine learning models trained on the collected features can identify new signals in real time, providing useful information for operating prosthetic devices, and other applications. Predictions allow for smooth interaction between users and assistive devices, improving usefulness and usability in clinical, rehabilitation, and everyday situations (Raez, 2016).

Table 1. Algorithm of the research

Algorithm 1 Two-Stage Forearm Muscle Signal Processing and Classification	
1.	Initialization:
2.	Setup EMG/EEG electrodes on the forearm for signal acquisition
3.	Ensure hardware components (preamplifier, Sallen-Key filter) are operational
4.	Requires
5.	Surface EMG and EEG signals from the forearm
6.	Preamplifier for signal boosting
7.	Sallen-Key filter for noise reduction
8.	Labeled dataset for CNN training
9.	Ensure hardware components (preamplifier, Sallen-Key filter) are operational
10.	Stage 1: Hardware-Based Signal Preprocessing
11.	Input: Raw EMG/EEG signals
12.	Output: Clean, filtered signals suitable for feature extraction and analysis
13.	Step 1.1: Signal Acquisition
14.	Preamplifier boosts weak EMG/EEG signals from surface electrodes.
15.	Ensure: Signals are amplified while preserving original signal integrity.
16.	Step 1.2: Signal Filtering
17.	Apply a Sallen-Key low-pass filter to remove unwanted frequencies and noise:
18.	EMG filter: Retain signals in the 20-200 Hz range.
19.	EEG filter: Retain alpha (8-12 Hz) and beta (13-30 Hz) wave frequencies.
20.	Stage 2: Machine Learning-Based Feature Extraction and Classification

21. **Input:** Clean, filtered EMG/EEG signals
22. **Output:** Predicted forearm muscle gestures
23. **Step 2.1: Transformation**
24. Apply Wavelet Transform and Fast Fourier Transform (FFT) to convert time-domain signals into the frequency domain for analysis.
25. **Step 2.2: Feature Extraction**
26. Extract time-domain features such as: Mean Absolute Value (MAV), RMean Absolute Value (MAV), Zero Crossings
27. Step 2.3: K-Means Clustering
28. Use K-means clustering to group similar signal frames. The clustering groups are based on the similarity in extracted features allowing identification of dominant muscle groups.
29. **Step 2.4: Classification (CNN)**
30. Train a Convolutional Neural Network (CNN) using the labeled dataset. The CNN automatically learns patterns to differentiate between muscle gestures.
31. Step 2.5: Gesture Prediction
32. Use the trained CNN model to classify real-time EMG/EEG signals and predict forearm muscle movements. The output is a real-time prediction of muscular gestures for controlling prosthetic devices or assistive technologies.

5.2. System Construction

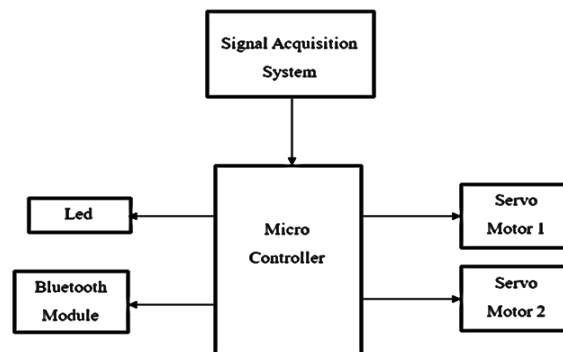


Figure 3. Block Diagram for System

The main objective is to analyze forearm low-dimensional data. In particular, the system is made to adjust to different bio-signal inputs, such as the detection of muscle movement. Because these signals are faint, proper data interpretation requires filtering and amplification. EMG measures electrical activity in muscles, with higher

signals indicating stronger contractions and more activated muscles. Effective signal processing is essential to isolate meaningful muscle activity from static noise, enabling precise analysis of forearm muscle function.

6. Result and Analysis

6.1. EMG and EEG Raw Dataset Time Series

Initially, the raw signal was quantized into 255 levels to determine the appropriate frequency response. The time-domain signal was then multiplied by a unit impulse response to identify the corresponding peak, which was compared against the frequency response. The deviation factor was calculated, and the impulse response was adjusted based on this factor. This process was iterated until the error response fell below 10%.

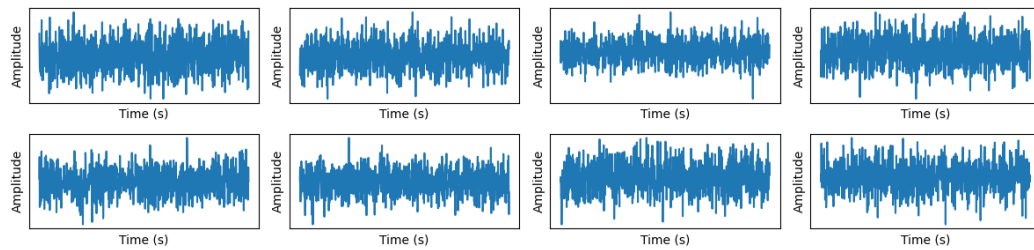


Figure 4: Raw Time Domain Data

6.2. Finding the Optimal Number of Clusters

According to the Elbow method, the optimal number of clusters is identified as the point where the rate of decrease in inertia begins to slow down. In this instance, the optimal number of clusters is determined to be 3.

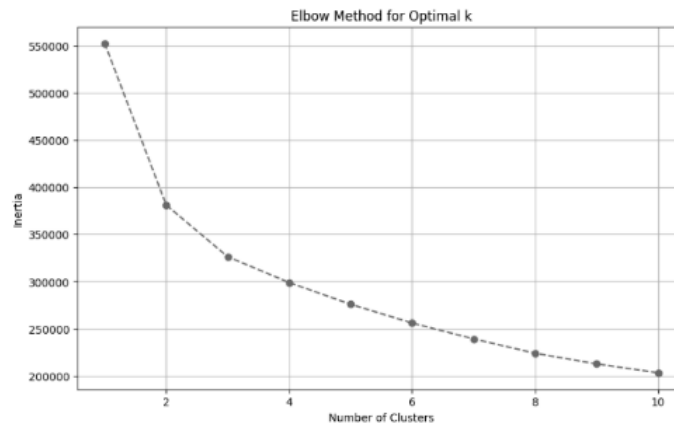


Figure 5: Optimal value of Cluster Calculation

The method for clustering is k-means clustering, with the optimal number of clusters determined to be 3 based on the Elbow method, where the inertia starts to decrease more slowly. PCA was applied for dimensionality reduction and visualization purposes, but the clustering itself was performed in the original feature space. The size and distribution of cluster #3 are a result of the data spread as assigned by the algorithm, not influenced by the scatter plot, which merely visualizes the reduced dimensions. According to the PCA analysis, muscle group A exhibits high and balanced cluster separation, while muscle group B shows moderate separation with slightly uneven cluster sizes. In contrast, muscle group C has low cluster separation and uneven cluster sizes.

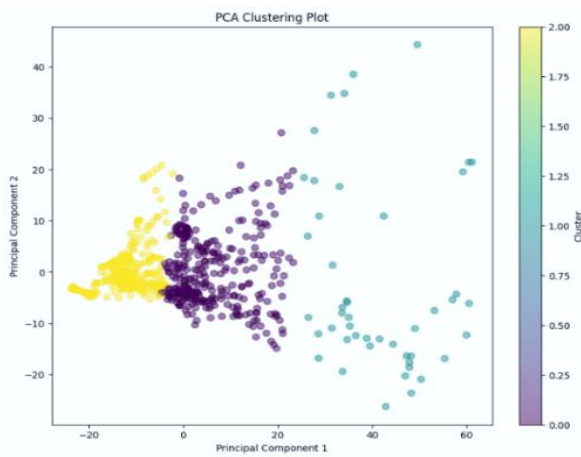


Figure 6: PCA for Optimal Clustering of dataset

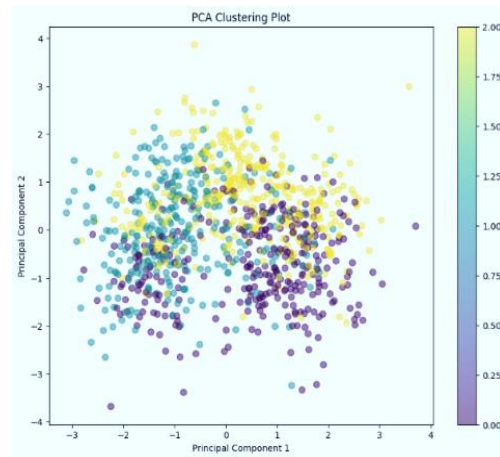


Figure 7: PCA for Optimal Clustering of muscle groups

Table 2. Cluster Comparison for Dataset and Actual Data

Muscle Group Dataset	Dataset Cluster Separations	Dataset Cluster Size	Dataset Cluster Shape	Actual Muscle Group	Actual Data Cluster Separations	Actual Data Cluster Size	Actual Data Cluster Shape
Muscle A	High	Balanced	Compact	Muscle A	High	Imbalance	Elongated
Muscle B	Moderate	Slightly imbalance	Compact	Muscle B	High	Slightly imbalance	Compact
Muscle C	Low	Imbalance	Spherical	Muscle C	Low	Imbalance	Compact

The imbalance of the cluster is due to

- Low SNR due to 50Hz interference signal (External Artifact)
- Lead Artifacts
- Sweat Artifacts
- Muscles Artifacts

Movement during EMG recording can introduce artifacts from adjacent or related muscle groups, which is a common issue in extracting accurate EMG signals.

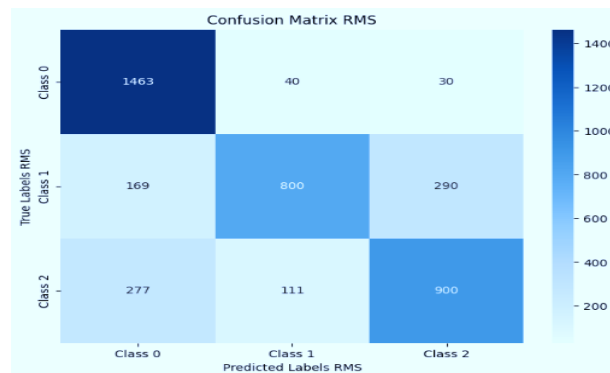


Figure 8: Confusion Matrix based on RMS

for Class 0, indicating that the model accurately detected 1463 occurrences of Class 0. The other cells show how many cases of Class 0 were wrongly classified as Class 1 and Class 2, respectively, and how soon. The model performs remarkably well in Class 0, with a large number of correct predictions and few misclassifications. For Class 1 and Class 2, the model continues to perform relatively well, though it shows a higher rate of misclassifications compared to Class 0.

7. Conclusion and Discussion

The paper focuses on the use of EEG and low-dimensional EMG signals for advanced signal processing and biofeedback from the forearm. The main goal is to study these biological signals to understand how they behave and change with different circumstances. To learn more about the patterns and features of pre-recorded biomedical signals, a thorough study of the signals was carried out. This required using advanced signal processing methods, such as band-pass filtering to separate important frequency components, differential amplification to strengthen weak EMG signals, and full-wave rectification along with smoothing to precisely estimate muscle activity. In order to classify and predict muscle group activations based on EMG and EEG signal patterns; the study utilized machine learning techniques. This method aims to increase the accuracy of the study of muscle function by utilizing machine learning's capacity to adjust to complex data.

Overall, the project demonstrates significant advancements in analyzing forearm EMG and EEG signals, providing valuable insights into muscle activity and neurological signals for research and clinical applications.

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